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From Nordin & Frankel (1989)

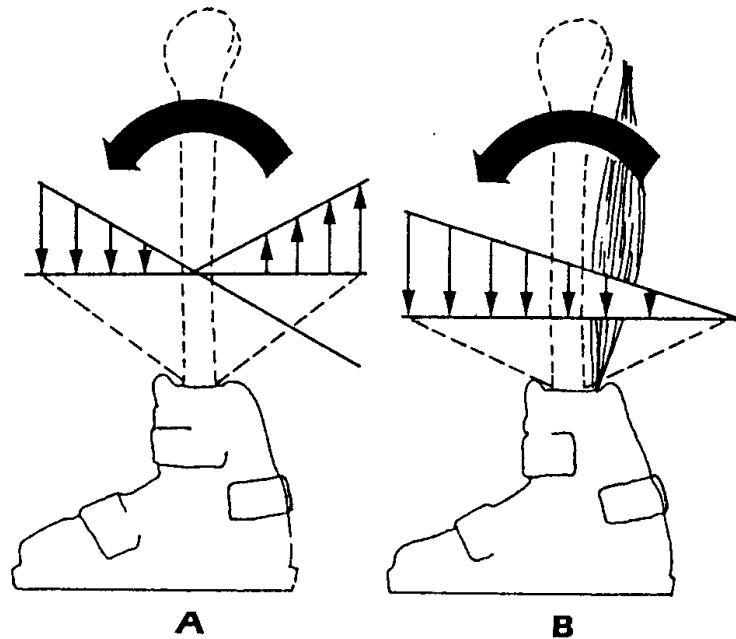


FIG. 1-31

**A.** Distribution of compressive and tensile stresses in a tibia subjected to three-point bending. **B.** Contraction of the triceps surae muscle produces high compressive stress on the posterior aspect, neutralizing the high tensile stress.

(12)

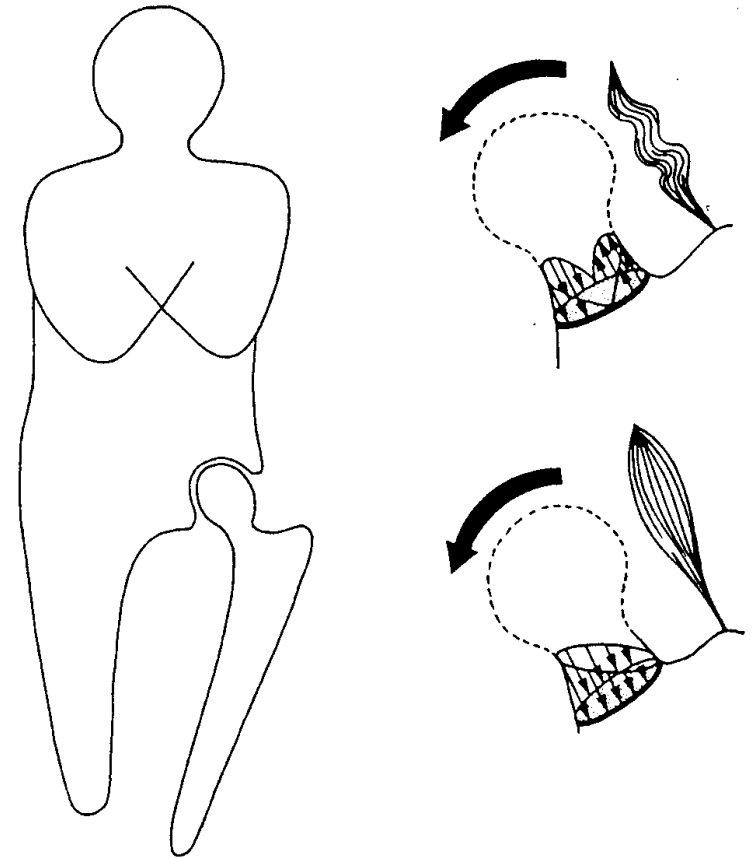


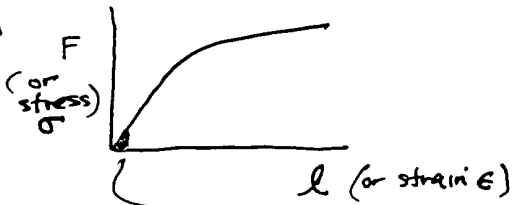
FIG. 1-32

Stress distribution in a femoral neck subjected to bending. When the gluteus medius muscle is relaxed (top), tensile stress acts on the superior cortex and compressive stress acts on the inferior cortex. Contraction of this muscle (bottom) neutralizes the tensile stress.

(13)

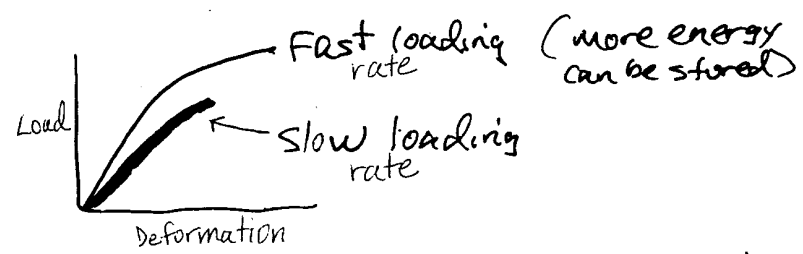
" " in bone during

loading



In Normal daily activities, the energy stored is a small fraction of what is needed to fracture a bone.

Faster and stronger — bone is stiffer and can absorb more energy

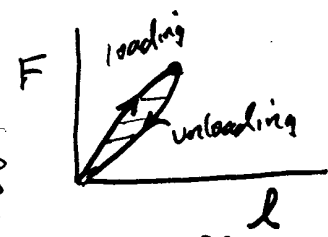


Risk from fractures at high speed loadings of small bone fragments injuring neighboring soft tissue as all this energy is released.

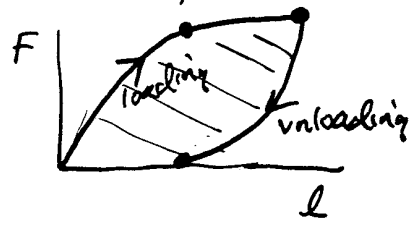
(14)

This does not occur as much in slow speed loading of bones. Here there tends to be a single crack with little displacement of bone pieces.

- energy loss during loading & unloading



below yield point



Hysteresis loop  $\Rightarrow$  area inside the loop represents the energy lost during the loading & unloading process

When loading is all the way to fracture, none of the energy is recovered and is lost to heat and permanent deformation as well as kinetic energy of bone fragments

Fatigue of bone under repetitive loading

The amount of load that can be tolerated before injury occurs gets as the number of reps increases

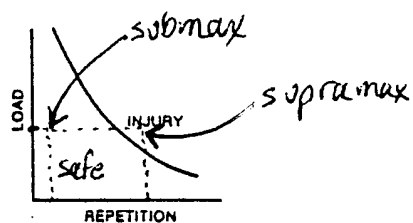


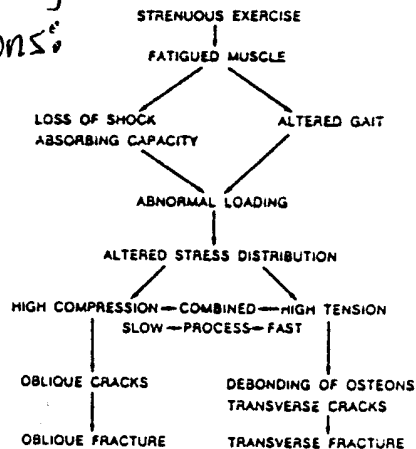
FIG. 1-36 The interplay of load and repetition is represented on a fatigue curve.

15

Wolff's Law: A bone will adapt to the loads that are placed on it (if given sufficient recovery time). The bone will become \_\_\_\_\_ (and be able to store \_\_\_\_\_ before failure) in response to the loads placed on it. Conversely - inactivity will do just the reverse. Take away the loads and over time the bone will get \_\_\_\_\_

16

Theoretical chain of events leading to injury during fatigue situations:



Influence of bone size & shape on strength & stiffness

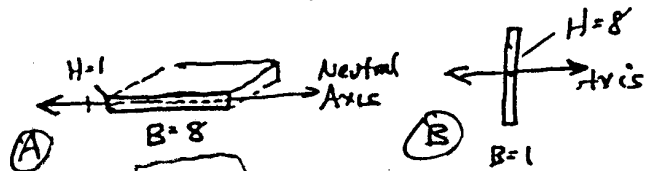
In tension & compression, cross-sectional area (X-sectional area) is the determining factor. Note stress = force/area ( $\sigma = F/A$ )

so \_\_\_\_\_  
 so for a given level of stress - increasing X-sectional will increase the force that the bone will tolerate.

In bending: Here the relevant factor is called \_\_\_\_\_. This quantity takes into account both X-sect. area and the distribution of material about

(17)

the neutral axis.



$I = \frac{BH^3}{12}$  for a rectangular x-section.

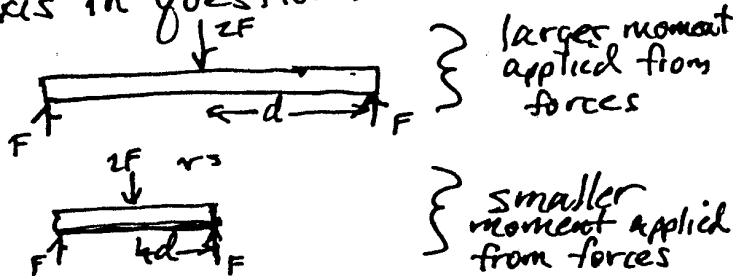
Case A:  
 $I = \frac{8 \times (1)^3}{12} = \frac{8}{12}$

Case B:  
 $I = \frac{1 \times (8)^3}{12} = \frac{512}{12}$

= 64 times as large as case A.

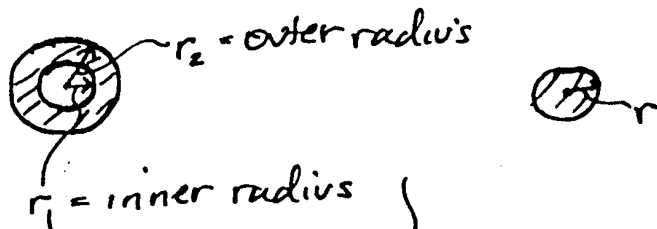
This area moment of inertia represents the \_\_\_\_\_

However the strength of the whole bone against bending moments also depends on the \_\_\_\_\_. The longer the bone is, the \_\_\_\_\_ the moment arm of a force applied distal to the joint axis in question.



(18)

Tubular material



(Hollow)

$I = \frac{\pi}{4} r_2^4 - \frac{\pi}{4} r_1^4$   
 equiv. solid x-section      hollow space

(Solid)

$I = \frac{\pi}{4} r^4$

For a given bending moment M applied to a structure

The stress depends on both the \_\_\_\_\_ and on the \_\_\_\_\_

stress  $\sigma = \frac{M a}{I}$   
 distance from neutral axis  
 area moment of inertia

Note: as "a" increases,  $\sigma$  \_\_\_\_\_  
 " M " ,  $\sigma$  \_\_\_\_\_  
 " I " ,  $\sigma$  \_\_\_\_\_  
 holding all else constant

Maximum stress ( $\sigma_0$ ) produced by a bending moment

$\sigma_0 = \frac{M r}{I}$  where  $r$  = outside radius or maximum distance from neutral axis

(for a round x-section)

for rectangular max value of  $a = \frac{M H}{2 I}$

General:  $\sigma_0 = \frac{M c}{I}$  where  $c$  is the max value of  $a$

See example of solid vs hollow bone problem

Torsion: Similar factors affect strength & stiffness in bones - However the relevant variable is called \_\_\_\_\_

\_\_\_\_\_ This describes how the material is distributed away from the neutral axis for torsion see Fig 1-39

$I_p$  = polar moment of inertia



Fracture healing -

After fracture - during the healing process - a cuff of callus forms around the site - increasing \_\_\_\_\_ (and hence strength to resist tension & compression loads), \_\_\_\_\_ moment of inertia (hence increasing strength to resist bending loads) and \_\_\_\_\_ moment of inertia (hence increasing strength to resist torsional loads). Then as healing is completed, the cuff is progressively \_\_\_\_\_.

Aging: with progressing age, there is a marked decrease in the total amount of bone tissue and a slight decrease in actual size of bones. Result: reduced strength and decrease in the length of the plastic region on the stress-strain curve (bone becomes \_\_\_\_\_).

Osteoporosis is a major problem with the elderly (from reduction in \_\_\_\_\_). Weight bearing loads are necessary to reduce the chances of osteoporosis. Exercise alone is \_\_\_\_\_.